

GW data analysis

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In this handout I describe some basic techniques in GW data analysis, partly following the descriptions given in [2] and [1].

1 Preliminaries

- the Fourier transform of a signal $x(t)$ and its inverse are defined by the formulas

$$\tilde{x}(f) = \int_{-\infty}^{+\infty} x(t) e^{-2\pi i f t} dt, \quad x(t) = \int_{-\infty}^{+\infty} \tilde{x}(f) e^{2\pi i f t} df \quad (1)$$

- the action of filters in the time domain is described by the convolution

$$(x * y)(t) = \int_{-\infty}^{+\infty} x(t') y(t - t') dt' \quad (2)$$

- consider the Fourier transform of the convolution of two signals $x(t)$ and $y(t)$ with Fourier transforms $\tilde{x}(f)$ and $\tilde{y}(f)$

$$\begin{aligned} \int_{-\infty}^{+\infty} (x * y)(t) e^{-2\pi i f t} dt &= \\ &= \int_{-\infty}^{+\infty} \left[\int_{-\infty}^{+\infty} x(t') y(t - t') dt' \right] e^{-2\pi i f t} dt \\ &= \int_{-\infty}^{+\infty} x(t') e^{-2\pi i f t'} dt' \int_{-\infty}^{+\infty} y(t - t') e^{-2\pi i f (t - t')} dt \\ &= \int_{-\infty}^{+\infty} x(t') e^{-2\pi i f t'} dt' \int_{-\infty}^{+\infty} y(t'') e^{-2\pi i f t''} dt'' \\ &= \tilde{x}(f) \tilde{y}(f) \quad (3) \end{aligned}$$

(convolution theorem)

- a process is *stationary* when all its statistics are constant in time, i.e., when its probability distribution is invariant with respect to time translations. A noise can be weakly stationary when only some of its statistics are time-invariant, for example only mean and variance.
- a process is *ergodic* when time averages are equal to ensemble averages.

- Parseval's theorem

$$\int_{-\infty}^{+\infty} x(t)y^*(t)dt = \int_{-\infty}^{+\infty} dt \int_{-\infty}^{+\infty} \tilde{x}(f')e^{2\pi i f' t} df' \int_{-\infty}^{+\infty} \tilde{y}^*(f'')e^{-2\pi i f'' t} df'' \quad (4)$$

$$= \int_{-\infty}^{+\infty} df' \int_{-\infty}^{+\infty} df'' \tilde{x}(f')\tilde{y}^*(f'') \int_{-\infty}^{+\infty} e^{2\pi i (f' - f'')t} dt \quad (5)$$

$$= \int_{-\infty}^{+\infty} df' \int_{-\infty}^{+\infty} df'' \tilde{x}(f')\tilde{y}^*(f'')\delta(f' - f'') \quad (6)$$

$$= \int_{-\infty}^{+\infty} \tilde{x}(f)\tilde{y}^*(f)df. \quad (7)$$

- the total square fluctuation of a real stationary signal $s(t)$ is given by

$$\int_{-\infty}^{+\infty} |s(t)|^2 dt = \int_{-\infty}^{+\infty} dt \left| \int_{-\infty}^{+\infty} \tilde{s}(f)e^{2\pi i f t} df \right|^2 \quad (8)$$

$$= \int_{-\infty}^{+\infty} df' \int_{-\infty}^{+\infty} df'' \tilde{s}(f')\tilde{s}^*(f'') \int_{-\infty}^{+\infty} e^{2\pi i (f' - f'')t} dt \quad (9)$$

$$= \int_{-\infty}^{+\infty} df' \int_{-\infty}^{+\infty} df'' \tilde{s}(f')\tilde{s}^*(f'')\delta(f' - f'') \quad (10)$$

$$= \int_{-\infty}^{+\infty} |\tilde{s}(f)|^2 df \quad (11)$$

(Plancherel formula). Notice that this is what physicists usually call Parseval's theorem

- the *power spectral density* (PSD) of a signal $s(t)$ is usually defined as follows

$$S(f) = \lim_{T \rightarrow \infty} \frac{1}{T} \left| \int_{-T/2}^{+T/2} s(t)e^{-2\pi i f t} dt \right|^2, \quad (12)$$

which is a *two-sided spectral density* where the frequency runs over negative as well as positive values. However, for real signals — as in the case of the $h(t)$ signal recorded by a GW IFO — the PSD is an even function, i.e., $S(-f) = S(f)$, and for this reason it is customary to define and use the *one-sided spectral density*

$$S^{(1)}(f) = \lim_{T \rightarrow \infty} \frac{2}{T} \left| \int_{-T/2}^{+T/2} s(t)e^{-2\pi i f t} dt \right|^2, \quad (13)$$

where $f \geq 0$.

- the definition is similar for a noise signal $n(t)$, the only difference is an ensemble average

$$S^{(1)}(f) = \lim_{T \rightarrow \infty} \frac{2}{T} \left\langle \left| \int_{-T/2}^{+T/2} n(t)e^{-2\pi i f t} dt \right|^2 \right\rangle, \quad (14)$$

which is again a one-sided spectral density.

- the autocorrelation function of a zero-mean stationary, ergodic process $s(t)$ is defined by

$$R(\tau) = \langle s(t)s(t+\tau) \rangle = \lim_{T \rightarrow \infty} \frac{1}{T} \int_{-T/2}^{+T/2} s(t)s(t+\tau) dt \quad (15)$$

Notice that here ergodicity is essential to substitute the ensemble average with a time average.

- autocorrelation function and PSD are closely related. Consider the PSD

$$S^{(1)}(f) = \lim_{T \rightarrow \infty} \frac{2}{T} \left| \int_{-T/2}^{+T/2} s(t)e^{-2\pi i f t} dt \right|^2 \quad (16)$$

$$= \lim_{T \rightarrow \infty} \frac{2}{T} \int_{-T/2}^{+T/2} s(t')e^{2\pi i f t'} dt' \int_{-T/2}^{+T/2} s(t)e^{-2\pi i f t} dt \quad (17)$$

Now let $t = t' + \tau$, so that $dt = d\tau$ in the second integral (where t' behaves as a constant), then we obtain

$$S^{(1)}(f) = \lim_{T \rightarrow \infty} \frac{2}{T} \int_{-T/2}^{+T/2} s(t')e^{2\pi i f t'} dt' \int_{-T/2}^{+T/2} s(t'+\tau)e^{-2\pi i f t'} e^{-2\pi i f \tau} d\tau \quad (18)$$

$$= \int_{-\infty}^{+\infty} e^{-2\pi i f \tau} d\tau \lim_{T \rightarrow \infty} \frac{2}{T} \int_{-T/2}^{+T/2} s(t')s(t'+\tau) dt' \quad (19)$$

$$= 2 \int_{-\infty}^{+\infty} R(\tau)e^{-2\pi i f \tau} d\tau \quad (20)$$

i.e., the PSD is the Fourier transform of the autocorrelation function (this is the *Wiener-Kintchine theorem*).

- if the noise is white, stationary and Gaussian, it is completely characterized by its variance N_0 in the time domain. When one takes a two-sided spectral representation, this means (from Plancherel's theorem) that

$$S(f) = \sigma^2 \quad (21)$$

2 Gaussian noise

By definition a sampled noise is Gaussian when the samples have a Gaussian distribution. Here we assume that samples of a Gaussian white noise process are taken with time step Δt , and that the variance of each sample is σ^2 , so that the correlation function is $R_{jk} = \langle x_j x_k \rangle = \sigma^2 \delta_{jk}$. Using a discretized version of the Wiener-Kintchine theorem, we find the single-sided PSD

$$S_x^{(1)}(f) \approx 2 \sum_{j=1, N} R_{0j} e^{2\pi i f(j\Delta t)} \Delta t = 2\sigma^2 \Delta t \quad (22)$$

The probability density function of each sample x_i is

$$p(x_i) = \frac{1}{\sqrt{2\pi\sigma^2}} \exp \left[-\frac{x_i^2}{2\sigma^2} \right], \quad (23)$$

therefore the the joint probability density function of N samples is

$$p(\{x_i\}) = \frac{1}{(2\pi\sigma^2)^{N/2}} \exp \left[-\frac{\sum_{i=1,N} x_i^2}{2\sigma^2} \right] = \frac{1}{(2\pi\sigma^2)^{N/2}} \exp \left[-\frac{\sum_{i=1,N} x_i^2 \Delta t}{2\sigma^2 \Delta t} \right] \quad (24)$$

$$\propto \exp \left[-\frac{1}{S_x^{(1)}} \int_{-\infty}^{+\infty} x^2(t) dt \right] \quad (25)$$

$$= \exp \left[-\int_{-\infty}^{+\infty} \frac{|\tilde{x}(f)|^2}{S_x^{(1)}} df \right] \quad (26)$$

Now notice that we can generate non-white noises by proper filtering of a white noise. In the time domain, the filtering operation is described by a convolution

$$y(t) = \int_{-\infty}^{+\infty} k(t-t')x(t')dt' \quad (27)$$

where $k(t)$ is the pulse response function of the filter and its Fourier transform $K(f)$ is the transfer function of the filter. Then, in the frequency domain, we find

$$\tilde{y}(f) = K(f)\tilde{x}(f) \quad (28)$$

from the convolution theorem: this implies that

$$S_y(f) = |K(f)|^2 S_x(f) \quad (29)$$

Therefore

$$\begin{aligned} p(\{x_i\}) &\propto \exp \left[-\int_{-\infty}^{+\infty} \frac{|\tilde{x}(f)|^2}{S_x} df \right] = \exp \left[-\int_{-\infty}^{+\infty} \frac{|K(f)|^2 |\tilde{x}(f)|^2}{|K(f)|^2 S_x} df \right] \\ &= \exp \left[-\int_{-\infty}^{+\infty} \frac{|\tilde{y}(f)|^2}{S_y(f)} df \right] \end{aligned} \quad (30)$$

and we see that the formula holds also for non-white noise.

Notice that the interferometer noise has a frequency-dependent spectral density (the noise is not white), and therefore equation (30) represents what actually happens with signals embedded in the interferometer noise, **which is the same for all signals and is obtained by averaging in a given time span of interest.**

In addition, we can use the last result for the argument of the exponential as a motivation to introduce a real-valued scalar product in this function space:

$$(x, y) = \int_{-\infty}^{+\infty} \frac{\tilde{x}(f)\tilde{y}^*(f) + \tilde{x}^*(f)\tilde{y}(f)}{S_n(f)} df = 2 \operatorname{Re} \int_{-\infty}^{+\infty} \frac{\tilde{x}(f)\tilde{y}^*(f)}{S_n(f)} df, \quad (31)$$

or

$$(x, y) = 4 \operatorname{Re} \int_0^{+\infty} \frac{\tilde{x}(f)\tilde{y}^*(f)}{S_n^{(1)}(f)} df, \quad (32)$$

when we use a single-sided spectral density, and $S_n(f)$ is the power spectral density of the interferometer noise, so that we can write the probability density of the noise process as a function of such a scalar product

$$p(\{x_i\}) \propto \exp \left[-\frac{(x, x)}{2} \right]. \quad (33)$$

3 Optimal detection statistic and Bayes' theorem

Recall that for two hypotheses – null hypothesis $\mathcal{H}_0$ and alternative hypothesis $\mathcal{H}_1$ – Bayes' theorem writes

$$P(\mathcal{H}_{0,1}|s) = \frac{P(s|\mathcal{H}_{0,1})P(\mathcal{H}_{0,1})}{P(s|\mathcal{H}_0)P(\mathcal{H}_0) + P(s|\mathcal{H}_1)P(\mathcal{H}_1)} \quad (34)$$

and given the data, we select the hypothesis that maximizes the posterior probability $P(\mathcal{H}_{0,1}|s)$, this is the Maximum A Posteriori (MAP) choice. We can also consider the *odds ratio*

$$\frac{P(\mathcal{H}_1|s)}{P(\mathcal{H}_0|s)} = \frac{P(s|\mathcal{H}_1)P(\mathcal{H}_1)}{P(s|\mathcal{H}_0)P(\mathcal{H}_0)} \quad (35)$$

which reduces to

$$\frac{P(\mathcal{H}_1|s)}{P(\mathcal{H}_0|s)} = \frac{P(s|\mathcal{H}_1)}{P(s|\mathcal{H}_0)} \quad (36)$$

if the prior probabilities of the null and of the alternative hypothesis are equal (in this case the odds ratio is called the *Bayes factor*). It is noteworthy that the Bayes factor is called the *likelihood ratio* in frequentist statistics, in which context it is shown to be the “most powerful test of size α ” (Neyman-Pearson lemma). Given that the logarithm is a monotonically increasing function, the argument works also for the log likelihood ratio.

4 Matched filters

The detection problem that we face in GW data analysis involves a null hypothesis where the signal is just noise, $s(t) = n(t)$, and an alternative hypothesis where the signal is given by the sum of a GW signal plus noise, $s(t) = n(t) + h(t)$, and $h(t)$ is a theoretical GW signal model that we are searching in our interferometer data.

Then, the likelihood ratio is

$$\Lambda = \frac{p(s|\mathcal{H}_1)}{p(s|\mathcal{H}_0)} = \exp \left\{ \frac{1}{2} [-(s-h, s-h) + (s, s)] \right\} = \exp [(s, h) - (h, h)/2]. \quad (37)$$

Since the likelihood ratio depends on data only through the (s, h) product, which is a log likelihood ratio, we conclude that this is the optimal detection statistic, i.e.,

$$(s, h) = 4 \operatorname{Re} \int_0^{+\infty} \frac{\tilde{s}(f)\tilde{h}^*(f)}{S_n^{(1)}(f)} df \quad (38)$$

where $S_n(f)$ is the noise PSD. Eq. (38) defines the *matched filter*.

Here we remark that in eq. (38) the expression $\tilde{s}(f)/\sqrt{S_n^{(1)}(f)}$ is the Fourier transform of the *whitened signal* and $\tilde{h}^*(f)/\sqrt{S_n^{(1)}(f)}$ is the *whitened filter transfer function* (do not forget that $h(t)$ is a given GW signal model).

Next, consider a generic filter and its action in the time domain

$$y(t) = \int_{-\infty}^{+\infty} x(t')k(t-t')dt' \quad (39)$$

where $k(t)$ is the pulse response function of the filter. As an example, we can take the RC filter which has an exponential pulse response function, represented in the left panel of figure 1. As illustrated in the figure, we see that because of the $-$ sign in front of t' the pulse response function is time reversed in the convolution integral.

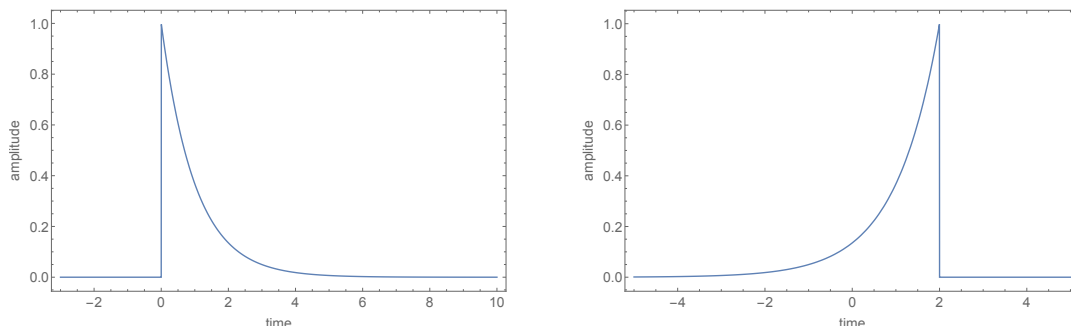


Figure 1: Left panel: pulse response function $k(t)$ of an RC filter; as in all causal filters, the pulse response function vanishes at negative times. Right panel: the pulse response function $k(t - t')$ acting on the signal in the convolution integral $\int_{-\infty}^{+\infty} x(t')k(t - t')dt'$, in this case for $t = 2$. We see that because of the $-$ sign in front of t' the pulse response function is time reversed in the convolution integral.

Now consider the inverse Fourier transform of the conjugate of a Fourier transform

$$\int_{-\infty}^{+\infty} \tilde{x}^*(f)e^{2\pi ift}df = \left[\int_{-\infty}^{+\infty} \tilde{x}(f)e^{2\pi if(-t)}df \right]^* = x(-t), \quad (40)$$

we find that it represents the time-reversed signal. Therefore, when we consider the matched filter defined in eq. (38), we see that it corresponds to a time convolution where the theoretical signal h is time-reversed. Overall, the theoretical signal is time-reversed twice, it is just the original signal, and the convolution corresponds to the sliding in time of the theoretical signal that acts like a template. The output of the matched filter is maximum when the template matches the experimental signal (see figures 2 and 3 for an illustration).

4.1 Signal-to-noise ratio (SNR)

Ideally, the matched filter has a template signal h that is equal to the detected signal s , and in that case

$$\rho_{\text{opt}}^2 = (h, h) = 4 \int_0^{+\infty} \frac{|\tilde{h}(f)|^2}{S_n^{(1)}(f)} df \quad (41)$$

which is the *optimal power signal-to-noise ratio*. The square root of the power SNR $\rho = \sqrt{\rho^2}$ is the *amplitude SNR*.

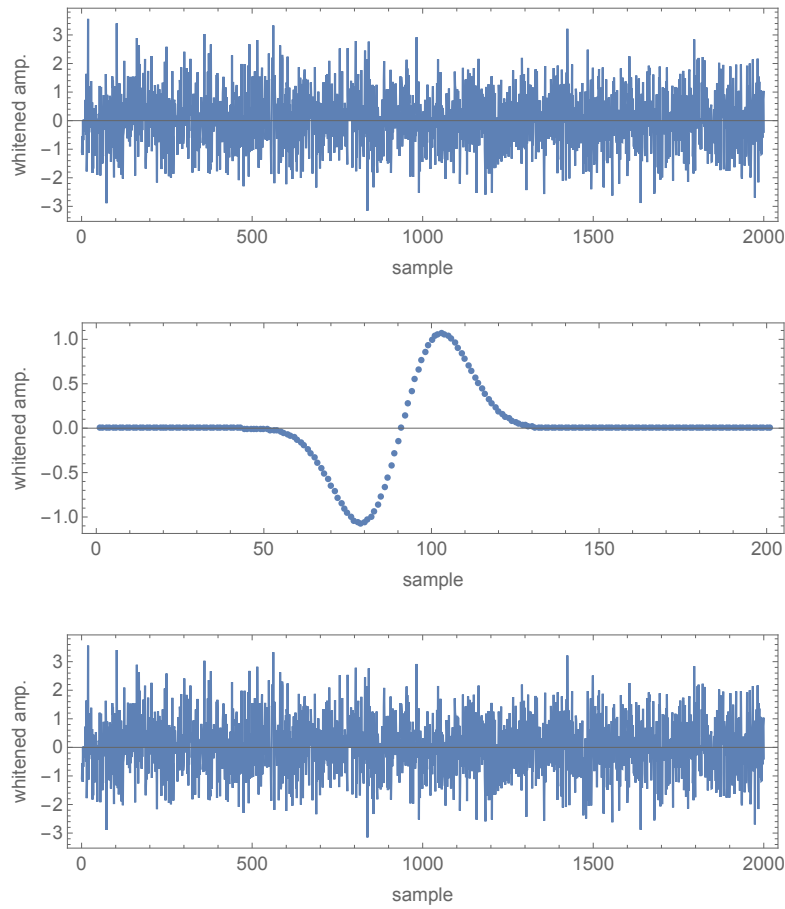


Figure 2: Consider the noise background shown in the top panel and the signal waveform in the middle panel. The waveform has been injected into (i.e., added to) the noise background with an unknown amplitude and the result is shown in the bottom panel. Can you see where the waveform has been injected?

References

- [1] Benjamin P Abbott, Rich Abbott, Thomas D Abbott, Sheelu Abraham, Fausto Acernese, Kendall Ackley, Carl Adams, Vaishali B Adya, Christoph Affeldt, Michalis Agathos, et al. A guide to LIGO–Virgo detector noise and extraction of transient gravitational-wave signals. *Classical and Quantum Gravity*, 37(5):055002, 2020.
- [2] Jolien DE Creighton and Warren G Anderson. *Gravitational-wave physics and astronomy: An introduction to theory, experiment and data analysis*. John Wiley & Sons, 2012.

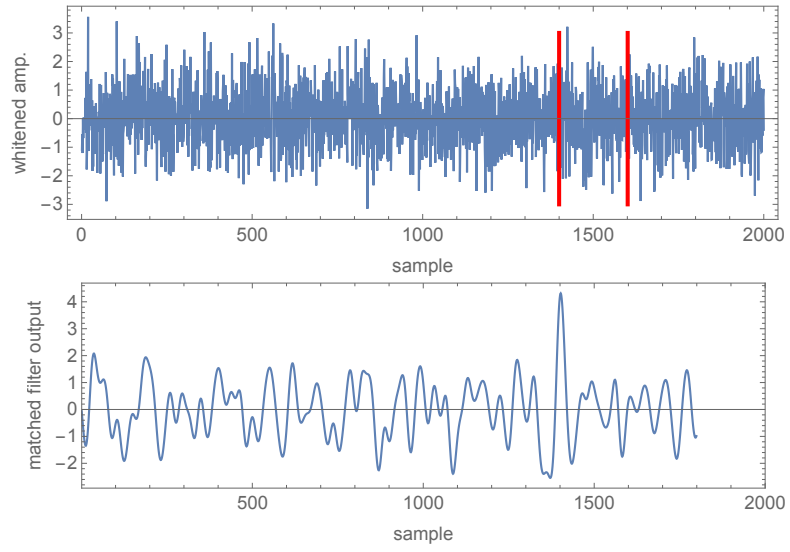


Figure 3: The upper panel is the same as the bottom panel of figure 2, but here the red bar show the region of injection of the signal into the noise background. The lower panel shows the output of the matched filter obtained by sliding in time the waveform shown in the top panel of figure 2. The peak shows the position of the start of the injection.